



Evaluation of Liposomal and Microbubbles Mediated Delivery of Doxorubicin in Two-Dimensional (2D) and Three-Dimensional (3D) Models for Breast Cancer

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ABSTRACT

Objective: Liposomal cancer treatment strategies are useful in removing the side effects that were the main concern in recent years. In this study, we prepared microbubble (MBs) conjugated with DOX-loaded liposomes (DOX-loaded MBs) and investigated their effectiveness in *in vitro* breast cancer cells in two dimensions (2D) and three dimensions (3D).

Materials and Methods: With this aim, breast cancer cells with different features (4T1, MDA-MB231, MCF-7) were grown in 2D and 3D dimensions. The cytotoxic and cell death effects under different conditions, durations and doses were evaluated with WST-1, trypan-blue, colony counts. Apoptotic effects were investigated with flow cytometric Annexin-V-PI and immunohistochemical (Ki-67, caspase 3, 8, 9) methods.

Results: After free DOX and LipoDOX were applied, the proliferation index of three cell lines reduced. Intrinsic and extrinsic apoptotic pathways were activated in both 2D and 3D models. However, this effect was observed at lower levels in the 3D model due to the difficulty of diffusion of DOX into the spheroids. Additionally, the suitability of the 3D model for breast cancer cells was supported by formation of ductus-like structures and spheroids. Cell deaths were not observed significantly with the DOX-loaded microbubbles due to rising of MBs to the surface and not reaching spheroids held in matrigel of 3D model.

Conclusion: DOX and LipoDOX showed anti-proliferative and apoptosis-inducing effects in breast cancer cells. However, these effects indicated variability depending on the cell lines and 2D or 3D model types.

Keywords: 3D cell culture, breast cancer, doxorubicin, liposome, microbubble

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Key Points

- Doxorubicin can be delivered with liposome and microbubbles.
- 3D spheroid model is suitable for *in vitro* breast cancer studies.
- 3D *in vitro* models are difficult to test microbubble loaded drugs.

Introduction

Cancer is one of the leading causes of deaths worldwide. In women, breast cancer is the most commonly diagnosed cancer. In fact, it is the second most common cause of cancer death among women (1, 2). In 2020, breast cancer accounted for ~ 684,000 deaths worldwide according to GLOBAACON (<https://doi.org/10.3322/caac.21660>). Several studies are being conducted to devise new strategies to overcome or reduce the common side effects associated with the administration of chemotherapeutics (3, 4). One of the strategies that is being widely explored involves the use liposomes to deliver entrapped cancer drugs. Commercially approved liposomal formulations include lipoplatin (cisplatin encapsulated in liposome) and LipoDOX [doxorubicin (DOX) entrapped in liposome] (5-7). Currently, the therapeutic safety and efficacy of LipoDOX for the treatment of triple-negative breast cancer is being evaluated in clinical trials and experimental studies in different combinations (8, 9). Most of the current research is focused using of poly (ADP-ribose) polymerase (PARP) inhibitors (10), in modified tandem peptide form (11), with liposomal immunotherapy (12), and in local gel form (13).

Microbubbles (MB), small gas-filled bubbles with size 0.5–10 µm, find wide applications in industry, medicine, and life sciences. Generally, microbubble shell structure is characterized by the presence of phospholipid with polyethylene glycol (PEG) as emulsifying agent. When

ultrasound is applied to MBs, the high pressure induces a compression movement resulting in the reduction in the size of MBs. Further, the reduction in pressure is accompanied by an increase in the size of MBs (14). Thus, the ultrasound images generated from the signals obtained from oscillations of microbubbles provide high quality and clearly comprehensible information. All these features make MBs a promising contrast agent for ultrasound imaging. During ultrasound imaging, the oscillation of MBs results in the development of transient pores in the cell walls. As the intensity of ultrasound increases, MBs form a jet flow. This results in the opening of holes in cell walls, allowing the flow of chemotherapeutic drug into the cells (15). Thus, MBs act as excellent drug delivery agents.

In the present study, the suitability of MBs as delivery agents for DOX was explored. Doxorubicin-loaded MBs were developed by attachment of DOX-loaded liposomes to ultrasound contrast agent microbubbles via avidin-biotin bridge. The study aimed to evaluate and compare the therapeutic efficacy of DOX-loaded MBs and DOX-loaded liposomes with free DOX in *in vitro* two-dimensional (2D) and three-dimensional (3D) models for breast cancer.

Material and Methods

Chemicals

Clinical grade liposomal doxorubicin (Caelyx LipoDOX) was purchased from Janssen Pharmaceutica NV, Belgium. Doxorubicin HCl (Adriamycin) India, was procured from West-Ward, Franco Indian Pharmaceuticals. Distearoyl glycerol phosphocholine (DSPC, 99%), 1,2 distearoyl glycerol 3 phosphoethanolamine N [methoxy(polyethylene glycol)2000] (DSPE-PEG2000), and biotinylated DSPE-PEG2000 were obtained from Avanti Polar Lipids (Alabaster AL). Cholesterol and polyoxyethylene-40-stearate (PEG40St) were purchased from Sigma Aldrich (St. Louis, MO).

Preparation and characterization of microbubbles, DOX-loaded liposomes (LipoDOX), and DOX-loaded MBs

Microbubbles were prepared using DSPC as lipid, (PEG40St) as emulsifier, and biotinylated DSPE-PEG2000. MBs were prepared using the process described previously by Onercan (16). Since Caelyx LipoDOX is not suitable for conjugation with MBs, LipoDOX was prepared in-house using a mixture of DSPC, cholesterol, DSPE-PEG, and biotinylated DSPE-PEG as described before (16). In order to prepare DOX-loaded MBs, preformed LipoDOX and MBs in same %50 weights were mixed and incubated for 15 min on a rotary mixer at room temperature. Unbound LipoDOX was removed from the solution by flotation technique. Unbound Lipodox was at bottom and MB loaded Lipodox was floating. The amount of DOX bound to the MBs was determined using a fluorescence spectrophotometer (SHIMADZU) with emission signal at 595 nm upon excitation

with a 470 nm laser. Characteristics for the various formulations used in the study are summarized in Table 1.

Formation of three-dimensional (3D) cell cultures and spherule diameter measurement

MCF-7 (HTB-22, ATCC) (hormone receptor positive human cell line), MDA-MB-231 (HTB-26, ATCC) (triple negative human cell line expressing human epidermal growth factor receptor 2 (HER2), non-amplified), and 4T1 (CRL-2539, ATCC) (triple negative mouse cell line) breast cancer cell lines were used in the study. The cells were cultivated using Dulbecco's Modified Eagle Medium, DMEM (Corning, 10-017 CV) for MDA-MB-231 and RPMI-1640 medium (Corning, 15-040 CV) for 4T1 and MCF7 supplemented with 1% L-glutamine (Corning, 25-005 CI), penicillin/streptomycin (Corning, 30-002-CI), and 10% fetal bovine serum (Corning, 35-010-CV). The cell lines were maintained at 37 °C in a humidified incubator under 5% CO₂. All the experiments were repeated thrice, at minimum three different time points.

For 3D cell culture, a Matrigel basement membrane matrix (Corning) was first brought to liquid state by incubation at 4 °C. The material was swirled to ensure proper dispersion of the material. In a 96 well plate, 1000 cells per well were seeded with Matrigel in 96 well plate, 6 wells per condition (17-19). The cells were incubated at 37 °C in a humidified incubator at 5% CO₂ for 24 hours. After 24 hours, the cells were treated with optimized doses of DOX, LipoDOX, and DOX-loaded MBs. For each treatment six wells were used. Samples were further incubated at 37 °C in a humidified incubator at 5% CO₂ for 48 hours. Post 48 hours, an inverted light microscope (LEICA DMIL) was used to image and count the number and diameter of spherules formed in each well. The cells were further stained with trypan blue to evaluate the number of live and dead cells. For trypan blue staining, 10 mL of the dye was added per 96 wells, media was removed, and number of blue and transparent cells were counted using a microscope. In addition to this, the cells seeded in 25 cm² flasks were treated with effective dose of DOX, LipoDOX, and DOX-loaded MBs for appropriate time and exposed to ultrasound. The cells without any treatment were used as controls for comparison. For immunohistochemical analysis, colonies were collected using a cell scraper and paraffin blocks were prepared. Immunohistochemical analysis was performed on the sections in 3D to evaluate the expression of Ki-67, caspase-3, caspase-8, and caspase-9.

This study was approved by Dokuz Eylül University, Noninvasive Ethics Committee (date: 09.11.2020, no: 2017/26-22).

Flow pattern

Breast cancer cells were grown on the surface of sterile slides inserted in a flask (4-well Multidish, Nunc). For 2D model, cells were directly seeded onto the slides at a cell density of 10,000 cell/ml. For *in vitro*

Table 1. Characterization results for various formulations used in the study

Sample	DOX concentration (mg/ml)	Sample	Concentration (MB/ml)	Mean size (mm)
LipoDOX	493.8	MB before conjugation	2.66×10^9	3.11
DOX-loaded MBs	15.4	MB after conjugation	7.90×10^8	2.99

LipoDOX: Doxorubicin (DOX) entrapped in liposome; MB: Microbubbles

3D studies, 21.8 cm²/well area was seeded with 10⁶ cells mixed in 1 mL of cold liquid Matrigel per unit surface. The cells were incubated at 37 °C to allow hardening of the Matrigel for 30 minutes. Further, complete medium was added and plate was incubated for 48 hours for spherule formation. After 48 hours, the cells were used for flow experiments. A special flow chamber was designed to perform the experiments in 2D and 3D. The cells were placed in the flow chamber and the flow experiments were performed. The MB loaded DOX were fluxed through the flowing apparatus over cells.

Measurement of cell proliferation using WST-1 assay

In a 96 well plate, the cells were seeded at a density of 10⁴ cells/well and treated with different doses of DOX and LipoDOX (0.5, 1.5, 2.5, 5, 10, and 20 µM). For each treatment six wells were used. Cell proliferation assay was performed after 24 and 48 hours of incubation using WST-1 solution (Roche, 11644807001). To evaluate the effect of dose and time on cell viability, the cells were treated with WST-1 at a concentration 10 µL/well and incubated at 37 °C for 1 hour. Cell proliferation was measured in terms of absorbance at 450 nm using an ELISA reader (Thermo). LD50 (50% Lethal dose) for DOX and LipoDOX on these breast cancer cell lines was calculated as [(absorbance of test sample - absorbance of control)/control].

Flow cytometry-based measurement of apoptosis and necroptosis using Annexin-V-FITC/PI staining

Post the treatment of cells with different formulations, treated and control cells were collected and centrifuged at 1,200 rpm for 5 min. The supernatant was carefully removed without disturbing the cell pellet. The resulting cell pellet was resuspended in 100 µL of PBS buffer. For FACS analysis, one tube for each sample without staining was used for gating. The remaining tubes were stained with propidium iodide (PI) alone, FITC-Annexin-V alone or combination of PI and Annexin-V (Sigma-Aldrich A9210). All the tubes were incubated for 15 minutes at 4 centigrade degree. After 15 minutes of incubation, binding buffer was added to each tube and flow cytometry analysis (BD-Accuri, C6 Flow Cytometer) was performed (FITC with FL 1 dedector at 530/30 nm filter and PI with FL2 dedector at 585/42 nm). After appropriate gating, early apoptotic and late apoptotic/necrotic cells were identified using Annexin-V staining alone and a combination of Annexin-V and PI, respectively. The data for flow cytometry analysis was expressed as percentage calculated in comparison to the initial cell counts.

TUNEL and immunohistochemistry

For each cell line, cells were seeded in a 25 cc flask and treated with LC50 doses (obtained in the previous assay) for 24 or 48 hours (time and dose for each treatment are given in results section). The cells were collected in 15 mL tubes and centrifuged at rpm. The supernatant was carefully removed and the cells were fixed by the addition of methanol. After 24 hours, the cells were blocked for tissue monitoring and paraffin blocking was performed. Sections of 5 µm thickness were placed on positive-loaded slides.

The sections were incubated in an oven at 60 °C overnight. Further, the sections were deparaffinized with water and TdT labeling was performed using Biotin d-UTP kit (Genscript L00290) according to the manufacturer's protocol. The resulting sections were further stained with diaminobenzidine, while background staining was performed using hematoxylin. In order to calculate % apoptosis, the number of brown positive cells were counted per 5,000 cells and normalized for total cell count. The identification of apoptotic cells was performed on the basis of the presence of double chain fractures.

For immunohistochemistry analysis, the samples were treated with primary antibody for Ki-67 (Elabscience, e-pp-24636), caspase-3 (Bioss, Bs-0081R), caspase-8 (Bioss, Bs-0052R), and caspase-9 (Bioss, Bs-0049R) for 30 minutes. This was followed by treatment with anti-rabbit haptoglobin related protein secondary antibody at 1:200 dilution in automatic immunohistochemistry staining device (Ventana Discovery). The treatment with diaminobenzidine resulted in dark brown color. During analysis, positivity was used as the sole criteria, while sample intensity was not considered. Number of positive and negative cells were counted and percentage was calculated. For background staining hematoxylin dye was used. All sections showed positive cell counts, and cells and colonies were imaged using a light microscope (Olympus, Germany).

Statistical analysis

Data are represented as mean ± standard deviation. Statistical analysis was performed using SPSS 22.0 program. Nonparametric tests were used for analysis and the results of the study were considered statistically significant for p<0.05.

Results

Cell proliferation assay using WST-1

The effect of DOX dose and duration of treatment on cell viability was evaluated in three breast cancer cell lines using WST-1. Each cell line was treated with six different concentrations of DOX (0.5, 1.5, 2.5, 5, 10, and 20 µg/mL) for 24 and 48 hours. As shown in Figure 1, the effective near LC50 dose for 4T1, MCF-7, and MDA-MB-231 cells was found to be 1.5, 1.5, and 3 µg/ml, respectively. Both 4T1 and MDA-MB-231 cell lines showed LC50 time of 48 hours, while MCF-7 was characterized by LC50 time of 24 hours (Figure 1).

To evaluate the effect of LipoDOX on cell viability, all three cell lines were treated with seven different doses of LipoDOX (0.1, 0.25, 0.5, 0.75, 1, 1.5, and 2 µg/ml) and LC50 time and dose were calculated. The effective near LC50 time and dose for 4T1 cells was 48 hours and 1.5 µg/ml, respectively. In comparison to this, MCF-7 and MDA-MB-231 showed lower LC50 doses of 0.75 µg/ml and 0.25 µg/ml, respectively, which were observed at LC50 time of 24 and 48 hours, respectively (Figure 2).

Assessment of spherule number and diameter in 3D matrigel model

To assess the number and diameter of spherules formed, the cells were grown in 3D Matrigel and treated with optimized doses of DOX, LipoDOX, and DOX-loaded MBs. After 48 hours of treatment, spherule formation was evaluated using light microscopy. Spheroids displayed significant variability in terms of size, diameter, and numbers. In the control group, large size spheroids with ductus structures were observed. Interestingly, spheroids formed in case of MDA-MB-231 cell were smaller in size as compared to the spheroids for MCF-7. In comparison to these, most successful and dense spheroid formation was observed in 4T1 cells, where large of number of spheroids were formed. The treatment of all the cell lines with DOX resulted in significant decrease in spheroid diameters as compared to the control cells. These DOX treated spheroids showed significant necrosis and apoptosis. In case of DOX treated MCF-7 cells, spheroids were preserved, however, they were smaller size. A lower apoptosis rate was observed in MCF-7 cells as compared to other cell lines, which was in agreement with the aforementioned observation. In comparison to this, DOX treatment in MDA-MB-231 cells resulted in fewer number

of spheroids that showed apoptotic morphology. For all three cell lines included in the study, spherule counts and diameter were significantly reduced post administration of DOX and LipoDOX. Mean values for number and diameter of spherules observed for different treatment groups are summarized in Table 2. Figure 3 shows microscopic images of the 3D spherules formed for three breast cancer cell lines.

Technical Issues associated with 3D model studies

After successful development of 3D culture models for three cell lines, paraffin blocks were prepared and spheroid morphologies were assessed using hematoxylin-eosin staining. In Matrigel matrix (Corning, 354234), the cells formed a specific structure around the spheroids which was similar to connective tissue. The occasional occurrence of

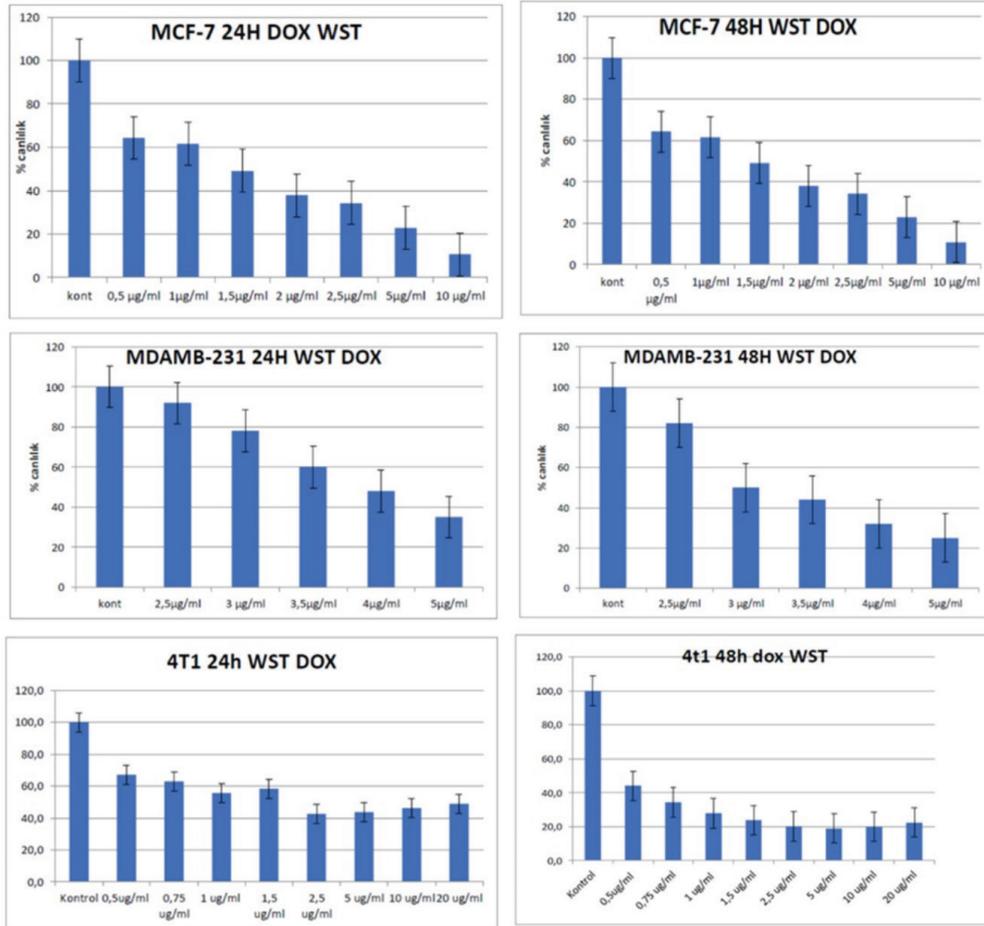


Figure 1. Doxorubicin WST-1 viability percentages compared with control in breast cancer cell lines. The effective near LD50 time and dose for 4T1 cells was 48 hours and 1.5 µg/ml, 24 hours and 1.5 µg/ml for MCF7 cells, 48 hours and 3 µg/ml for MDAMB-231 cells (p<0.05).

Table 2. Mean spherule number and diameters obtained in 3D cell culture model for three cancer cell lines. Mean spherule number and diameter were found to be reduced in DOX and LipoDOX treated groups as compared to control group, for all three cell lines (p<0.05)

3D Matrigel model	Mean spherule number	Standard derivation	Mean spherule diameter (µm)	Standard derivation
4T1 control	302	±18	306.2	±80.4
4T1 DOX	43	±8	104.4	±95.5
4T1 LipoDOX	82	±13	152.2	±46.2
MCF-7 control	338	±21	336.3	±90.1
MCF-7 DOX	182	±36	184.01	±50.8
MCF-7 LipoDOX	118	±42	227.04	±67.1
MDA-MB-231 control	286	±28	280.06	±120.8
MDA-MB-231 DOX	27	±7	76.21	±20.7
MDA-MB-231 LipoDOX	46	±15	117.01	±71.2

LipoDOX: Doxorubicin (DOX) entrapped in liposome; MB: Microbubbles

apoptotic objects in the center of the spheroids and ductus structures was quite significant, particularly in MCF-7. These observations provided evidence for the suitability of the structures formed in 3D cultures for breast cancer studies. The ductus structures were found to be located in the center of the spheroids.

In 4T1 cells, the number of spheroids were higher as compared to other two cell lines. The treatment of cells with DOX resulted in a reduction in spheroid diameters and cell counts per spheroid. However, the cell viability was found to be higher in 4T1 cells as compared to other cells in 3D model. Post DOX treatment, 4T1 cells in 3D model were characterized by disrupted and reduced ductus structures. All three cell lines exhibited high proliferation index in 3D cell cultures. However, the identification of 3D model proliferation index was difficult as compared to 2D cultures.

The treatment of cells with DOX-loaded MBs failed to produce any results. This was mainly attributed by rising of MBs to the surface that remained under the Matrigel and did not diffuse owing to their large size. DOX dissolved in the medium could easily diffuse through the pores of the Matrigel and bound to the cells; however, the spheroids formed above the Matrigel did not allow the transition of liposomes

and MBs into the pores. As a result, DOX-loaded MBs did not pass through the pores and failed to reach the cells. Therefore, DOX-loaded MBs were not included in the following proliferation and apoptosis experiments.

For all three cell lines, the decrease in mean spherule number and diameter upon treatment with DOX and LipoDOX was found to be statistically significant as studied using Mann-Whitney U test ($p < 0.05$).

Flow pattern findings

The flow experiments were successfully performed in 2D model; however, 3D model could not be used for flow pattern studies owing to the inability of the drug to enter the spherules. DOX and LipoDOX were successfully applied to the cells in 2D model. A model to perform shear stress formulation was adapted. Results for the same will be provided in our future studies. One of the aims of the flow experiments was to utilize ultrasound to burst the MBs near the cells. This would have allowed the release of DOX from the liposomes, while the formation of transient pores in the cells by sonoporation would have assisted in the passage of the drug molecules. However, the experiment could not be performed as the MBs added to the

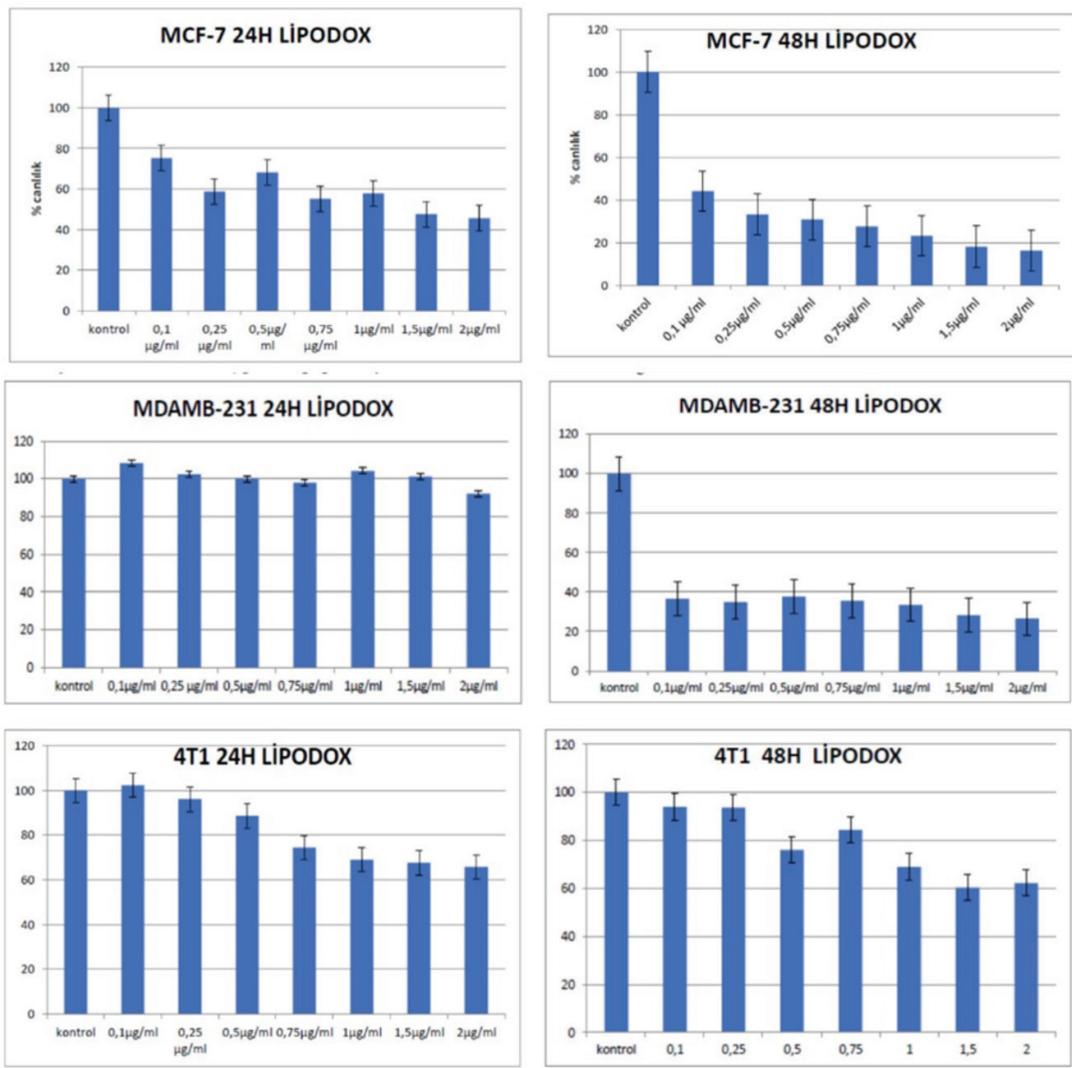


Figure 2. Liposomal-Doxorubicin WST-1 viability percentage compared with control in breast cancer cell lines. The effective near LD50 time and dose as 48 hours and 1.5 µg/ml for 4T1 cells, 24 hours and 0.75 µg/ml for MCF7 cells, 48 hours and 0.25 µg/ml for MDAMB-231 cells ($p < 0.05$).

medium for ultrasound destruction floated. As a result, these MBs did not contact the cells on the surface and failed to show any significant binding.

Apoptosis and necroptosis findings with flow cytometric Annexin-V-FITC/PI staining

The cells were treated with DOX and LipoDOX using the effective LC50 dose and time optimized in the previous experiments. Post treatment, the cells were collected, stained with Annexin-V-FITC/PI, and assessed using flow cytometry. The treatment of the three breast cancer cells with DOX and LipoDOX using optimized dose and incubation time resulted in the induction of cell death via necrosis (Table 3). For DOX treatment, the necrosis rate was found to be 95.5%–99.1%, while LipoDOX showed necrosis rate of 75.8%–87.4%. Mann-Whitney U analysis displayed statistically significant difference among control, DOX, and LipoDOX groups for all the cell lines ($p < 0.05$).

TUNEL and immunohistochemistry findings

In 3D model studies, terminal deoxynucleotidyl transferase dUTP nick end labeling (TUNEL) staining was used for the identification

of apoptosis in the cells. For 3D model of 4T1 cells, 3% and 35% apoptosis was observed in the control and DOX treated groups, respectively (Table 4). Similar increase in apoptosis was observed for MCF-7 cells with DOX treatment, where apoptosis of 5% and 25% was observed in the control and DOX treated cells, respectively. In case of MDA-MB-231 cells, DOX treatment resulted in an increase in apoptosis to 24%. The treatment of the cells with LipoDOX was also accompanied by an increase in apoptosis, however, the rate of apoptosis was low as compared to free DOX. The involvement of both extrinsic and intrinsic pathways in this DOX induced apoptotic effect could be deciphered by the evaluation of caspase expression. In addition to this, significant morphological changes along with necrosis were also observed in DOX treated cells. When the results of 3D and 2D models were compared, significant differences were observed in proliferation indices and caspase levels.

In 4T1 cells, mouse-derived progressive triple-negative breast cancer cells, Ki-67 analysis showed high proliferative activity of 80% which reduced to 27.2% after treatment with DOX. In case of 3D cultures for 4T1 cells, the expression of caspase-3, 8, and 9 increased by 20%, 40%, and 20%, respectively, as compared to the control cells. 2D cultures for MDA-MB-231 cells showed a reduction in

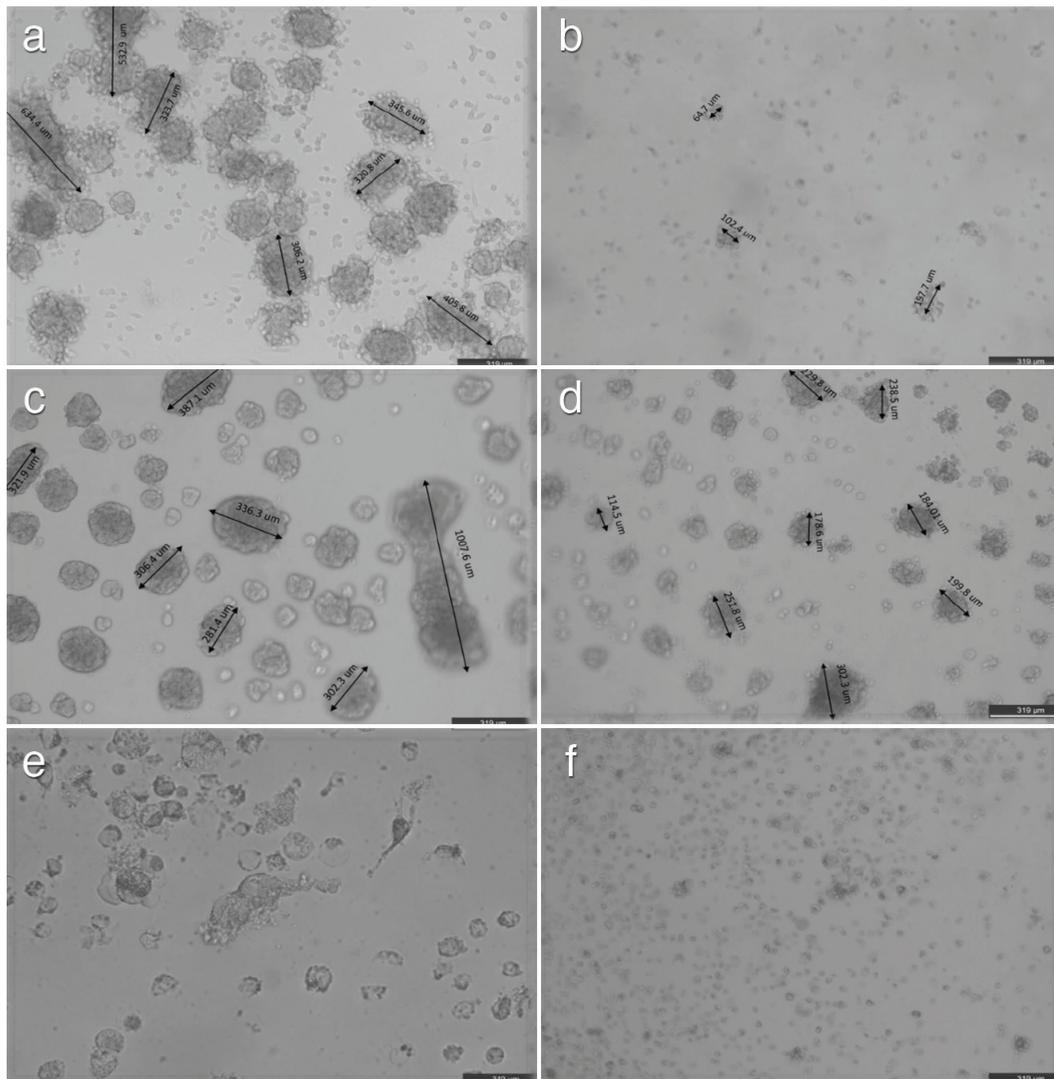


Figure 3. 3D Spherules in cell culture of **a)** Control 4T1 cells, **b)** DOX 4T1 cells; **c)** Control MCF7 cells, **d)** DOX MCF7 cells; **e)** control MDAMB231 cells and **f)** DOX MDAMB231 cells. Spherule number and diameters are prominently decreased in three cell lines after DOX incubation

3D: Three-dimensional; DOX: Doxorubicin

Ki-67 proliferation index from 98% to 13% upon treatment with DOX, while a significant increase was observed in the expression of caspase-3, 8, and 9. A comparative analysis for the three caspases showed maximum increase in case of caspase-8, indicating induction of both extrinsic and intrinsic pathways of apoptosis upon DOX treatment, but the activation of extrinsic pathway was comparatively higher.

In MDA-MB-231 cells, the activation of expression of caspase-3, 8, and 9 and reduction of proliferation index on DOX treatment was more significant as compared to 4T1 cells. These two cell lines are characterized by the presence of triple-negative breast cancer features. However, they differ in terms of their origin, one belongs to humans while the other is derived from mice. In human-derived MDA-MB-231 cells, DOX was found to be more effective in 2D cultures and its apoptosis-inducing effect was mediated via both extrinsic and intrinsic pathways. For MCF-7 cells, the increase in the expression

of caspase-3, 8, and 9 expressions was lower as compared to 4T1 and MDA-MB-231 cells.

In 3D spheroid model for 4T1 cell line, DOX treatment reduced Ki-67 proliferation index by 40%; however, the expression of caspase-3, 8, and 9 was higher in the control group. Higher expression of caspases in the control group of 3D models might be attributed to lower support provided by the Matrigel, which could have induced cell death in spheroids after certain duration owing to the absence of suitable vascularization. Additionally, identification of negative cells in terms of caspase expression within the spheroids indicated absence of any issue in immunohistochemical staining. In order to identify the apoptosis mechanism induced by DOX treatment, expression of caspase-3, 8, and 9 was evaluated, which are indicative of involvement of common apoptotic, extrinsic, and intrinsic pathways, respectively. Similar to 2D model studies, caspase-3, 8, and 9 were activated in 3D model for all three cells. However, in case of 3D model studies, the control groups

Table 3. Flow Cytometry results for the effect of DOX and LipoDOX treatment for three cancer cell lines used in the study. Both DOX and LipoDOX induced cell death majorly via necrosis for all three cell lines (p<0.05)

%	Viability AnnexinV-PI-	Early apoptosis AnnexinV +	Late apoptosis AnnexinV + PI +	Necrosis PI +
4T1 control	61.6	0.2	14.9	23.3
4T1 DOX	0.2	0.0	0.6	99.1
4T1 LipoDOX	21	2	1.2	75.8
MCF-7 control	46.8	0.3	1.3	51.6
MCF-7 DOX	2.0	0.0	2.7	95.3
MCF-7 LipoDOX	17.2	1	0.6	81.2
MDA-MB-231 control	78	0.0	5.6	16.4
MDA-MB-231DOX	1.5	0.3	8.4	89.8
MDA-MB-231 LipoDOX	4.6	2.8	5.2	87.4

Annexin-V (-) and PI (-) cells are indicative of viability, Annexin-V (+) PI (-) cells represent early apoptotic cells, Annexin-V (+) and PI (+) cells indicate late apoptotic cells, and only PI (+) cells are necrotic
LipoDOX: Doxorubicin (DOX) entrapped in liposome; MB: Microbubbles

Table 4. TUNEL and Immunohistochemistry results for 3D cell culture of breast cancer cell lines. Proliferation index was measured in terms of Ki-67, which decreased upon treatment of the cells with DOX and LipoDOX (p<0.05) as compared to the control, for all three cell lines used in the study. Activation of both intrinsic and extrinsic pathways was involved in the induction of apoptosis

%	TUNEL	Ki-67	Caspase-3	Caspase-8	Caspase-9
4T1 control	3	80	60	50	30
4T1 DOX	35	27	80	90	50
4T1 LipoDOX	23	50	100	100	85
MCF-7 control	5	80	30	49	20
MCF-7 DOX	25	19	60	82	81
MCF-7 LipoDOX	18	80	95	95	95
MDA-MB-231 control	6	98	36	21	21
MDA-MB-231 DOX	24	13	95	96	90
MDA-MB-231 LipoDOX	15	50	100	73	70

TUNEL: Terminal deoxynucleotidyl transferase dUTP nick end labeling; LipoDOX: Doxorubicin (DOX) entrapped in liposome; MB: Microbubbles

showed higher levels of expression for caspase-3, 8, and 9 as compared to 2D cultures. The treatment of MCF-7 cells with DOX resulted in 15% higher activation of caspase-3, 8, and 9 as compared to the control cells in 3D model. In addition to this, a 20% reduction in proliferation index was observed post DOX treatment. For MDA-MB-231 cells, DOX treatment in 3D cell cultures resulted in a lower reduction in the proliferative index as compared to 2D model. In 3D model studies, the proliferation index for all three cell lines was observed to reduce after DOX treatment. This reduction in proliferation for 3D models was low as compared to the reduction observed in 2D cell culture models. Thus, all these results are indicative of the reduction in intracellular diffusion of DOX in 3D cell culture model, which further highlights the suitability of 3D cell cultures for drug efficacy studies.

Discussion and Conclusion

2D cell culture models generally fail to mimic true *in vivo* tumor conditions (17, 18). In addition to this, 2D models generate very limited knowledge regarding the therapeutic efficacy of chemotherapeutic drugs. These limitations can be overcome by the use of 3D cell culture models. In comparison to 2D cultures, 3D cell culture models mimic *in vivo* tumor microenvironment in a much better way (17, 19). Several previous studies have reported significant differences in the results obtained for 2D and 3D cell culture models, particularly for the expression of various proteins and effects of chemotherapeutic drugs (19, 20). Similar results were obtained in the present study, where the expression of Ki-67, caspase-3, caspase-8, and caspase-9 in 2D cell cultures was comparatively low as compared to their 3D counterparts, irrespective of the cell line used for the evaluation.

In the present study, DOX and LipoDOX showed better 2D and 3D efficacy with increase in dose, for all the three cell lines studied. The observed change in efficacy was induced by the activation of apoptosis, particularly via induction of caspase-8. This was accompanied by a decrease in proliferative activity and viability in the 3D model, where significant reduction was observed in three-dimensional growth of the tumor cells. Moreover, the effective doses of LipoDOX required for the induction of cell proliferation inhibition and cell death were comparatively low as compared to free DOX, for all breast cancer cell lines used in the study. Thus, all these results suggest that lower doses of DOX would be safe for healthy cells, while ensuring effective inhibition of growth in breast cancer cells.

In the present study, the results obtained from the imaging studies highlighted the suitability of 3D cultures for breast cancer studies. In Matrigel matrix, the cells formed a structure similar to connective tissue around the spheroids. The occasional occurrence of apoptotic objects in the center of the spheroids and ductus structures was quite significant, especially in MCF-7 cells. These results were in agreement with a previous study, where establishment of spheroid like 3D model of breast cancer cell lines was associated with lower sensitivity toward chemotherapeutic drugs (18). These structures provided evidence for the suitability of the structures formed in 3D cultures for breast cancer studies.

In the present study, when spheroid structures were formed in 3D Matrigel model, DOX showed very limited diffusion into the cells, which was similar to *in vivo* conditions. Such a situation might be one of the responsible for the requirement of repeated administration of DOX at certain intervals under *in vivo* conditions. DOX showed antiproliferative and apoptosis-inducing effect in both 2D and 3D

models for all three cell lines used in the study; however, this effect was quite variable among the three cell lines. These findings might preclinically reflect the difference in treatment responses observed in different individuals diagnosed with same cancer type. This further highlights the importance of personalized therapy for cancer treatment.

The present study was associated with certain limitations. In 3D models, great difficulty was witnessed while evaluating proliferation of spheroids using absorbance-based WST-1. Thus, trypan blue staining might be more effective and reliable for testing viability of spheroids in 3D cell culture models. Since DOX is characterized by absorbance maxima of 480 nm, it might interfere with the absorbance-based measurements performed using WST-1.

In the present study, the effects of DOX and LipoDOX treatment on three different breast cancer cell lines were investigated in 2D and 3D cell culture models. Both drug formulations were found to be effective in all three breast cancer cells tested. The currently used strategies mainly focus on utilizing tumor targeting drug delivery vehicles to ensure local delivery of the drugs to the tissue of interest. Such targeted delivery minimizes the side effects and improves the antitumoral effect of the drug. In the present study, DOX-loaded MBs were targeted to the tumor cells by Epidermal growth factor receptor (EGFR); however, *in vitro* flow experiments could not be performed owing to the buoyancy of the MBs. The results for the antitumoral effects of DOX and LipoDOX obtained in the present study have laid down the foundation of a future study that will focus on the development of liposomal DOX-MB complex targeted specifically to breast cancer using EGFR. This study will also evaluate the local delivery of DOX in mouse model both in the presence and absence of ultrasound. Thus, the present study provided a suitable method for the evaluation of anti-proliferative and anti-apoptotic effects of liposomal doxorubicin in 3D cell culture models with different types of breast cancer cells.

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Informed Consent: This study is done on cell lines so that it does not require consent form

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Author Contributions

Conception: M.A., S.A.; Design: S.A., S.K.; Supervision: S.A., E.O., S.K.; Resources: M.A., S.A., E.O., Z.A., S.K.; Data Collection and/or Processing: M.A., S.A., S.K.; Analysis and/or Interpretation: M.A., S.A., S.K.; Literature Search: M.A., S.A., Z.A., S.K.; Writing Manuscript: M.A., S.A., Z.A., S.K.; Critical Review: S.A., S.K.O, E.O.

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